Analysis of Contours of Tumor Masses in Mammograms by Higuchi's Fractal Dimension

ROBERT STĘPIEŃ*, PAWEŁ STĘPIEŃ

Nalęcz Institute of Biocybernetics and Biomedical Engineering, Polish Academy of Sciences, Warsaw, Poland

We have tested a new method of assessment of mammographic images for medical diagnosis to differentiate between benign masses and malignant breast tumors. 2-D image is preprocessed to form 1-D signature of the image contour and then its complexity is analyzed using the Higuchi's fractal dimension method. We prove that the Higuchi's fractal dimension, $\mathbf{D}_{f,s}$ is a good classifier enabling differentiation between malignant tumors and benign masses.

K e y w o r d s: fractal dimension, breast cancer, image analysis

1. Introduction

Mammography is a popular X-rays technique for early diagnosis of breast cancer. This technique is often used in screening for detection of tumor masses. After detecting a tumor mass in mammogram, biopsy is needed for checking the kind of the tumor, whether it is benign or malignant tumor. The tissue from biopsy is examined by a pathologist. The biopsy is an invasive and time demanding method. Recently, many studies are devoted to find quick noninvasive methods based on mammographic images for classification of breast tumors. Several methods of image analysis were tested $[1\div7]$. The techniques based on fractal analysis are among them $[8\div15]$.

Fractal analysis can be a very useful method for quantitative assessment and classification of many kinds of medical images [16÷17]. R. M. Rangayyan and T. M. Nguyen tested some fractal analysis methods on images of breast tumor masses to differentiate between malignant and benign tumors. They computed fractal

^{*} Correspondence to: Robert Stępień, Nałęcz Institute of Biocybernetics and Biomedical Engineering, Polish Academy of Sciences, ul. Ks. Trojdena 4, 02-109 Warsaw, Poland, e-mail: rstepien@ibib.waw.pl

Received 27 October 2009; accepted 06 May 2010

dimension of contours of breast masses obtained from mammographic images either directly from the 2-D contour or from the 1-D 'signature' derived from the contour; they applied either the 1-D ruler method or the box counting method [8]. Again, we propose to use the Higuchi's method for analysis of '*signatures'* – the method is simpler than the other fractal methods and leads to comparable results.

2. Methods

The Higuchi's fractal dimension (D_f) is calculated directly from the data series, without embedding the data in a phase space [18]. It is, in fact, fractal dimension of the curve representing the series, and so it is always between 1 and 2, since a simple curve has, dimension equal 1 and a plane has dimension equal 2. The fractional part of D_f is a measure of the series complexity. It should not be misled with fractal dimension of an attractor in the system's phase space.

There are few ways to obtain signatures from image contour. In presented study we used the following methods. The contour of an image is specified in any rectangular coordinate system, i.e. by the set of pairs (x_i, y_i) such that pairs i - 1, i, i + 1 correspond to consecutive points on the contour for any i = 1, ..., N; the first point i = 1 may be chosen arbitrary and the point i = N + 1 coincides with the point i = 1 i.e. the contour is a closed planar curve.

We calculate arithmetic averages, x_0 and y_0 , of coordinates of all contour points and transform rectangular coordinates into polar ones; it is enough to calculate *r*-coordinate:

$$r_{i} = \sqrt{\left(x_{i} - x_{0}\right)^{2} + \left(y_{i} - y_{0}\right)^{2}}.$$
(1)

The series r_i is a 1-D 'signature' of the 2-D contour and we analyze the signatures of breast masses contours using the Higuchi's method.

We tested the Higuchi's fractal dimension, D_f , as a classifier for breast masses to benign or malignant tumors categories. We checked effectiveness of D_f for distinguishing benign masses from malignant tumors by analyzing a ROC curve [19÷21] (Receiver Operating Characteristic; plot *Sensitivity* against 1-*Specificity*). We calculate the Higuchi's fractal dimensions, D_f , from the whole signature.

3. Data

Two main data sets of contours of breast masses were used in this study both supplied to us by Prof. R.M.Rangayyan (University of Calgary, Alberta, Canada). The diagnostic classification of the masses was based upon biopsy. The contour of each mass was manually drawn by an expert radiologist specialized in mammography and verified independently by another radiologist.

Most of the benign masses in the data set 1 (DS1) are well-circumscribed (circumscribed benign or CB) (Fig. 1a), whereas most of the malignant tumors are spiculated (spiculated malignant or SM) (Fig. 1b), as typically encountered in mammographic images. The data set DS1 contains the contours of the 57 masses.



Fig. 1. Contours of a circumscribed benign (CB) mass (a) and of a spiculated malignant (SM) breast tumor (b) their signatures (c and d respectively; cf. Eq. (1)) and the signatures' Higuchi's fractal dimension (e and f respectively). Signature of malignant tumors shows lower fractal dimension (f) than that of a benign mass (e)

The data set 2 (DS2) includes circumscribed and spiculated cases in both the benign and malignant categories. SB (spiculated benign) masses and CM (circumscribed malignant) tumors are unusual, and tend to cause difficulties in pattern classification studies. The data set DS2 contains the contours of the 54 masses.

It is created a third data set, for global statistic. The combined data set (CDS) was prepared by combining all cases in the first and the second data sets.

The results obtained are presented for the three data sets (first and second data sets separately and combined) to demonstrate the strengths and weaknesses of the Higuchi fractal dimension method when used in characterizing of the breast masses and the tumors of various types. More information about the data contains paper of R. M. Rangayyan and T. M. Nguyen [8].

4. Results and Discussion

We calculated the average Higuchi's fractal dimension for the data sets DS1 and DS2. In the data set DS1 37 benign masses had average D_f equal 1.3 ± 0.14 . (mean \pm standard deviation). The remaining 20 masses were malignant tumors with the average Higuchi's D_f was equal 1.07 ± 0.05 . In the data set DS2, the average D_f of 28 benign masses was equal 1.13 ± 0.11 and average D_f of 26 malignant tumors was 1.05 ± 0.3 .

While contour of a circumscribed benign breast mass (Fig. 1a) seems to be more regular than contour of a spiculated malignant breast tumor (Fig. 1b), fractal dimension of the malignant breast tumors is lower than fractal dimension of the benign breast masses. If the contours were magnified one observed that these of the benign masses showed much more small irregularities than those of the malignant tumors. That is why signature of benign mass shows many small 'fluctuations' while that of malignant tumor does not (cf. Fig. 1a and Fig. 1b, respectively), so leading to differences in their fractal dimension. Problem of calculation of the length of coast-line considered by Mandelbrot [22] is quite analogous. In fact, fractal dimension turned out to be the best characteristics that actually gives possibility to compare properties of different coast-lines .

For assessment performance of the Highuchi's fractal dimension for differentiation of benign from malignant tumor analysis of Receiver Operating Characteristic curve (ROC) [19÷21] was used. In a ROC graph true positive rate (TPR, Sensitivity), is plotted *vs.* false positive rate (FPR, 1 – Specificity) for different cut-off points. Definitions of TPR, FPR, Sensitivity, and Specificity are as follows:

TPR = true positive results of test/all positive results of test FPR = false positive results/all negative results of test Sensitivity = TPR

Specificity = true negative results/all negative results of test

Each point of the ROC curve represents a sensitivity/specificity pair corresponding to a particular decision threshold. The better test's performance is for curve closer

52

to the upper left corner of the graph. So, performance obtained for the data set DS1 was much better than for the data set DS2 (Fig. 2). Table 1 contains cut-off points for the best sensitivity and specificity calculated for all studied data sets.

The area under the ROC curve (AUC - Area Under Curve) is a general indicator of quality of the test. Summarized results of AUC are contained in Table 2.



Fig. 2. ROC curves indicating the classification performance of Higuchi's fractal dimension for Data Set 1 (DS1), Data Set 2 (DS2), Combined Data Set (CDS). The area under ROC curve, AUC, for these data sets DS1, DS2 and CDS are 0.96, 0.7, and 0.84, respectively (Table 2)

Table 1. The optima	l cut-off points for best	performance of the test
---------------------	---------------------------	-------------------------

Data set	Cut-off point for the best sensitivity and specificity		
DS1	1.14		
DS2	1.11		
CDS	1.11		
Circumscribed masses (subset of data set 2)	1.11		
Spiculated masses (subset of data set 2)	1.03		

Table 2. The results of quality of the test by area under ROC curve, AUC

Data set	AUC – area under ROC curve	Standard error of AUC	95% confidence interval	Z statistic	Significant level P p-value
DS1	0.96	0.03	0.872 to 0.994	18.715	0.0001
DS2	0.70	0.07	0.562 to 0.819	2.846	0.0044
CDS	0.84	0.04	0.759 to 0.903	9.228	0.0001
Circumscribed masses (subset of data set 2)	0.92	0.07	0.722 to 0.990	7.025	0.0001
Spiculated masses (subset of data set 2)	0.58	0.11	0.393 to 0.757	0.793	0.428

The *p*-value (Table 2) showed ability of D_f to distinguish between benign and malignant masses. If *p* is significantly smaller then 0.05 then AUC is significantly different from 0.5 and therefore there is an evidence that the fractal dimension can distinguish the malignant masses from the benign masses. For the data set DS1 the test based on D_f was excellent; for the combined data set, CDS, the test was good. But for DS2 the test was only fair, because this set containing circumscribed masses and the second subset containing spiculated masses then we can see why the test is only fair. The average D_f of the circumscribed benign masses was equal 1.2 ± 0.09 and D_f of the malignant tumors was equal 1.07 ± 0.03 so the result was similar to values obtained for data set 1. The area under the ROC curve AUC = 0.92. These results are better than for CDS and close to the results obtained for DS1.



Fig. 3. ROC curves indicating the classification performance of Higuchi's fractal dimension for circumscribed and speculated subsets of Data Set 2. AUC for spiculated masses is not statistically greater than 0.5 so it is not possible to distinguish benign from malignant tumor by values of D_f

The result of analysis of AUC (Table 2) showed that D_f classifier did not differentiate benign masses from malignant tumors for the subset of spiculated masses (last row in Table 2). The average values of D_f were the same for the benign and for the malignant tumors – for the spiculated masses were equal 1.03. When we took cut-off value for CDS, equal 1.11 (Table 1), all spiculated cases were indicated as the malignant tumors. AUC for the spiculated masses were not statistically greater then 0.5 so it was not possible to distinguish the spiculated benign from the spiculated malignant tumor by values of D_f . The performance of clinical test for the spiculated masses.

The Higuchi's fractal dimension shows accuracy comparable to the fractal dimension estimated with the 1D ruler method [8]. Furthermore, D_f is more accurate classifier for circumscribed masses; however it is poor in classification of atypical SB masses. The classification performance for masses of D_f is comparable to the other shape feature such as compactness [6], fractional concavity [7], spiculation index [5] and Fourier factor [6], which were compared with FD by R. M. Rangayyan and T. M. Nguyen [8].

5. Conclusions

The Higuchi's fractal dimension, D_f , is a good classifier of malignant tumors and benign tumors for circumscribed masses, while D_f shows poor classification performance for spiculated masses. The tests for spiculated shape of masses are usually false positives. The Highuchi's fractal dimension well classifies circumscribed masses while the 1D ruler method well classifies speculated masses. So, these two methods combined well classifies all tumor masses.

Acknowledgments

We thank Prof. R.M.Rangayyan (University of Calgary, Alberta, Canada) for data of contours of breast masses, used for calculations. This work was supported by IBBE PAS statutory activity 4.4/st/09.

References

- Rangayyan R.M., El-Faramawy N.M., Desautels J.E.L., Alim O.A.: Measures of acutance and shape for classification of breast tumors. IEEE Trans. Med. Imag. 1997, 16(6), 799Y810.
- Mudigonda N.R., Rangayyan R.M., Desautels J.E.L.: Gradient and texture analysis for the classification of mammographic masses. IEEE Trans. Med. Imag. 2000, 19(10), 1032Y1043, 2000.
- Sahiner B.S., Chan H.P., Petrick N., Helvie M.A., Hadjiiski L.M.: Improvement of mammographic mass characterization using spiculation measures and morphological features. Med. Phys. 2001, 28(7), 1455Y1465.
- Mudigonda N.R., Rangayyan R.M., Desautels J.E.L.: Detection of breast masses in mammograms by density slicing and texture flow-field analysis. IEEE Trans. Med. Imag. 2001, 20(12), 1215Y 1227.
- Rangayyan R.M., Mudigonda N.R., Desautels J.E.L.: Boundary modelling and shape analysis methods for classification of mammographic masses. Med. Biol. Eng. Comput. 2000, 38, 487Y496.
- Shen L., Rangayyan R.M., Desautels J.E.L.: Detection and classification of mammographic calcifications. Int. J. Pattern Recogn. Artif. Intell. 1993, 7(6), 1403Y1416.
- Alto H., Rangayyan R.M., Desautels J.E.L.: Content-based retrieval and analysis of mammographic masses. J. Electron. Imaging 2005, 14(2),1Y17.
- Rangayyan R.M., Nguyen T.M.: Fractal Analysis of Contours of Breast Masses in Mammograms, J. Digit. Imag. 2007, 20, 3 (September), 223–237.
- Matsubara T., Fujita H., Kasai S., Goto M., Tani Y., Hara T., Endo T.: Development of new schemes for detection and analysis of mammographic masses. In: Proc. 1997 IASTED International Confe-

rence on Intelligent Information Systems (IIS"97), Grand Bahama Island, Bahamas, December 1997, 63Y66.

- Pohlman S., Powell K.A., Obuchowski N.A., Chilcote W.A., Grundfest-Broniatowski S.: Quantitative classification of breast tumors in digitized mammograms. Med. Phys. 1996, 23(8), 1337Y1345.
- 11. Dey P., Mohanty S.K.: Fractal dimensions of breast lesions on cytology smears. Diagn. Cytopathol. 2003, 29(2), 85Y86, 2003.
- 12. Zheng L., Chan A.K.: An artificial intelligent algorithm for tumor detection in screening mammogram. IEEE Trans. Med. Imag. 2001, 20(7), 559Y567.
- Guo Q., Ruiz V., Shao J., Guo F.: A novel approach to mass abnormality detection in mammographic images. In: Proc. IASTED International Conference on Biomedical Engineering, Innsbruck, Austria, February 2005, 180Y185.
- Caldwell C.B., Stapleton S.J., Holdsworth D.W., Jong R.A., Weiser W.J., Cooke G., Yaffe M.J.: Characterization of mammographic parenchymal pattern by fractal dimension. Phys. Med. Biol. 1990, 35(2), 235Y247.
- Byng J.W., Boyd N.F., Fishell E., Jong R.A., Yaffe M.J.: Automated analysis of mammographic densities. Phys. Med. Biol. 1996, 41:909Y923.
- Mattfeldt T.: Spatial Pattern Analysis using Chaos Theory: A Nonlinear Deterministic Approachto the Histological Texture of Tumours. In: Losa G.A., Merlini D., Nonnenmacher T.F., Weibel E.R. (Eds.): Fractals in Biology and Medicine 1997, Birkhäuser, Basel, Boston, Berlin Vol. II, 50–72.
- Klonowski W.: Signal and Image Analysis Using Chaos Theory and Fractal Geometry. Machine Graphics & Vision 2004, 9, 403–431.
- Higuchi T.: Approach to an irregular time series on the basis of the fractal theory. Physica D 1988, 31, 277–283.
- 19. Metz C.E.: Basic principles of ROC analysis. Seminars in Nuclear Medicine 1978, 8, 283–298.
- Zweig M.H., Campbell G.: Receiver-operating characteristic (ROC) plots: a fundamental tool in clinical medicine. Clin. Chem. 1993, 39, 561–577.
- Griner P.F., Mayewski R.J., Mushlin A.I., Greenland P.: Selection and interpretation of diagnostic tests and procedures. Ann. Inter. Med. 1981, 94, 555–600.
- 22. Mandelbrot B.B.: How long is the coast of Britain? Statistical self-similarity and fractal, Dimension. Science 1967, 155, 636–638.